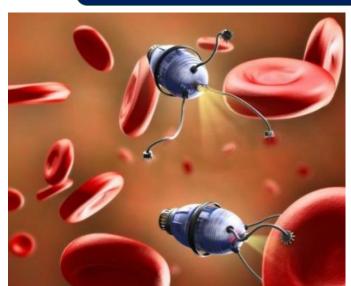
Torque and Force-Free Swimming at Low Reynolds Number

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Introduction and Background

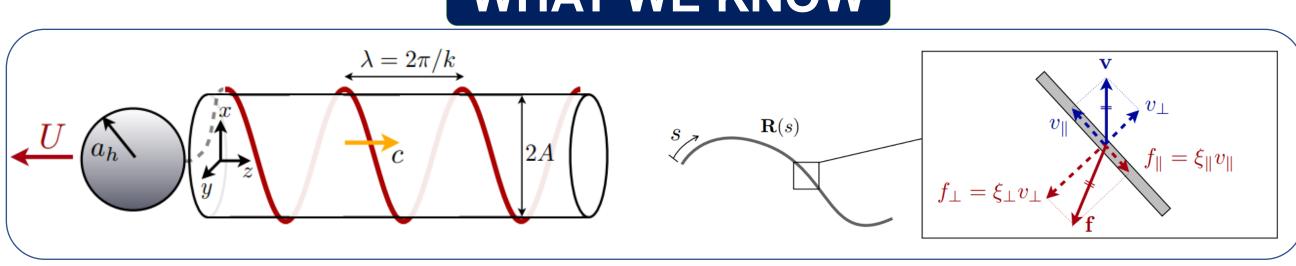
WHY STUDY MICROSWIMMERS?



Artificial bacteria are strong candidates for biomedical applications such as drug delivery and minimally invasive surgery

- ✓ Reduced side effects
- √ Faster recovery
- ? Swimming at small scales & in biological fluids is challenging!
- $Re = \frac{inertial\ forces}{viscous\ forces} = \frac{\rho UL}{\mu} \to 0$
- Biological fluids are complex fluids

WHAT WE KNOW



$$\mathbf{f}_{\text{vis}} = -[\xi_{\perp} \mathbf{n} \mathbf{n} + \xi_{\parallel} \mathbf{t} \mathbf{t}] \cdot \mathbf{v}, \quad \xi_{\perp} = \frac{2\mu\pi}{\ln(\frac{L}{r}) - 1/2}, \quad \xi_{\parallel} = \frac{4\mu\pi}{\ln(\frac{L}{r}) + 1/2}$$

$$\mathbf{v} = \mathbf{v}_d + \mathbf{U} + \mathbf{\Omega} \times \mathbf{r}$$

$$\mathbf{v}_{d} = \frac{\partial \mathbf{r}}{\partial t} = [A\omega \sin(k\alpha s - \omega t), -A\omega \cos(k\alpha s - \omega t), 0]$$

$$\mathbf{F}_{vis} = \int_{0}^{L} \mathbf{f}_{vis} ds, \quad \mathbf{M}_{vis} = \int_{0}^{L} \mathbf{r} \times \mathbf{f}_{vis} ds$$

$$\mathbf{F}_{vis} \cdot \mathbf{e}_{z} + F_{head} = 0, \quad F_{head} = 6\pi\mu a_{h} U$$

$$\mathbf{M}_{vis} \cdot \mathbf{e}_{z} + M_{head} = 0, \quad F_{head} = -8\pi\mu a_{h}^{3} \Omega$$

WHAT IS MISSING

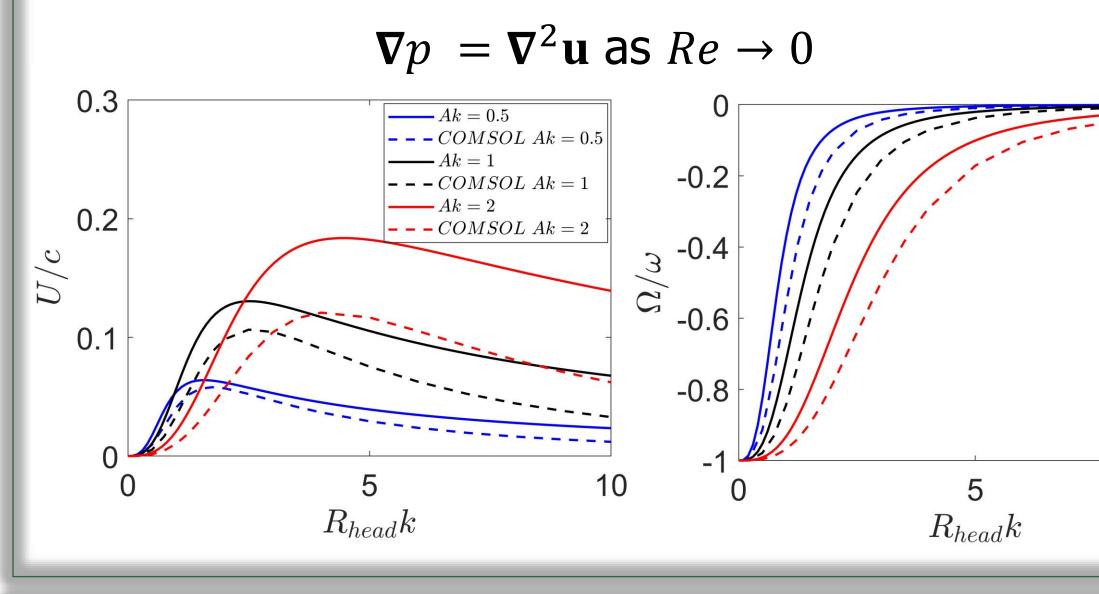
? Hydrodynamic interactions

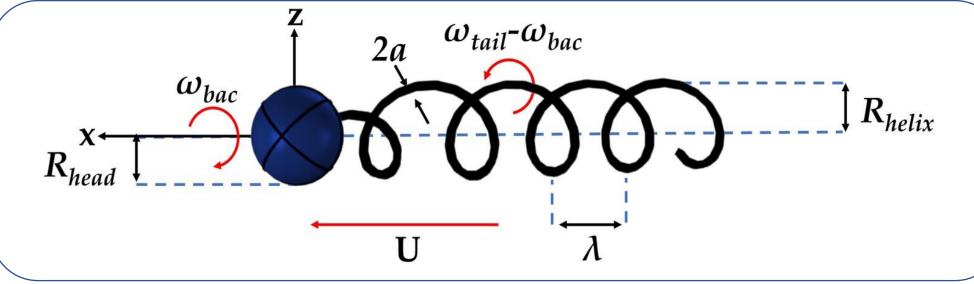
- Slender body assumption used in Pak & Lauga [1] does not take hydrodynamic interactions between helical turns, and tail and head into account
- ? Nonlinear effects
 - Slender body theory assumes that force and torque are linear combinations of velocity and angular velocity
- ? Effects of shear-thinning rheology
 - Most bodily fluids are shear-thinning!

CFD Model: Governing Equations and Validation

NEWTONIAN

$$Re\left(\frac{\partial \mathbf{u}}{\partial \mathbf{t}} + \mathbf{u} \cdot \nabla \mathbf{u}\right) = -\nabla p + \nabla^2 \mathbf{u}$$





$$\nabla p = \nabla \cdot \mathbf{\tau} \qquad \nabla \cdot \mathbf{u} = 0$$

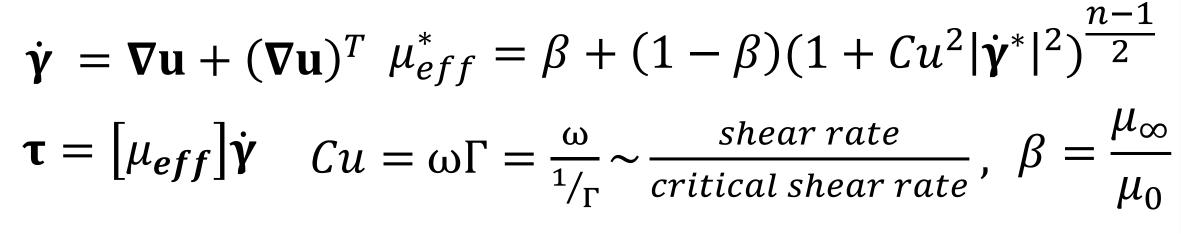
$$\mathbf{u} = \mathbf{U} + \mathbf{\Omega} \times (\mathbf{r} - \mathbf{r}_0), \quad \mathbf{r} \in S$$

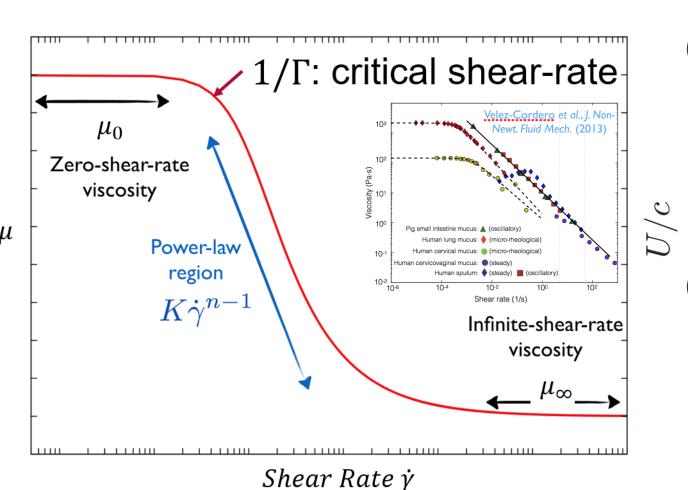
$$\mathbf{F}_{net} = \int_{S} \mathbf{\sigma} \cdot \mathbf{n} dA = \mathbf{0}$$

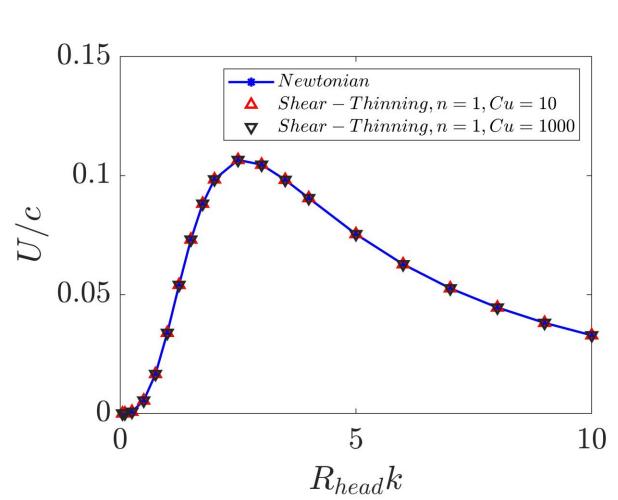
$$\mathbf{T}_{net} = \int_{S} (\mathbf{r} - \mathbf{r}_0) \times \mathbf{\sigma} \cdot \mathbf{n} dA = \mathbf{0}$$

$$\eta = \frac{\eta_{tug}}{\eta_{guire}}$$

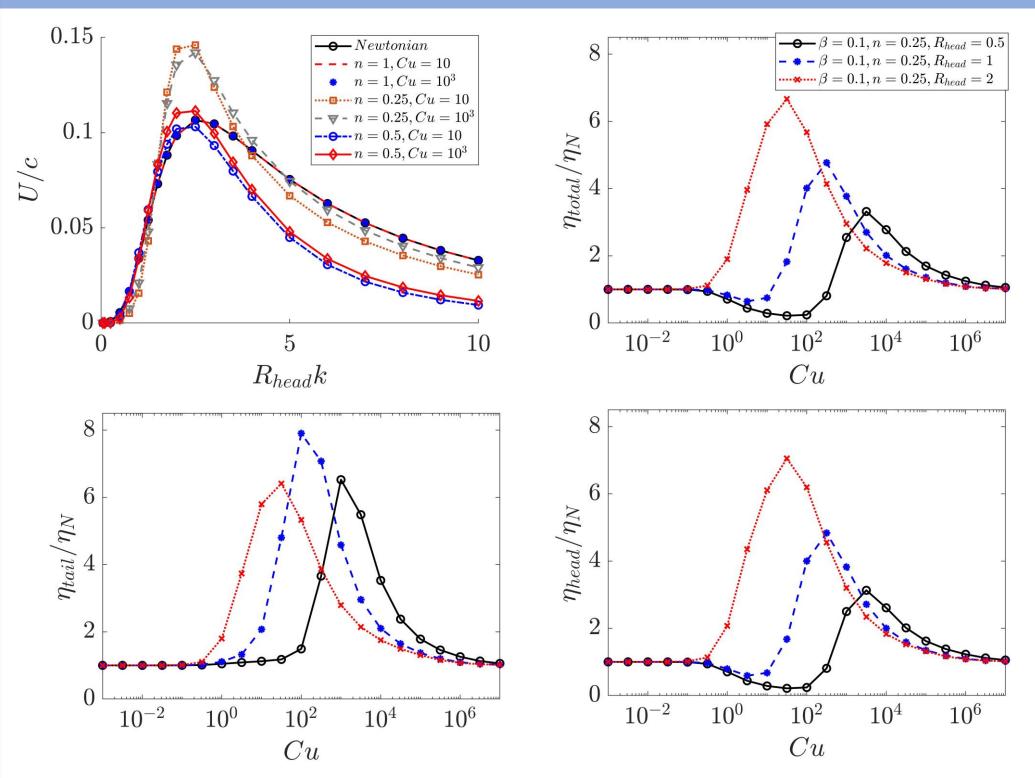
SHEAR-THINNING



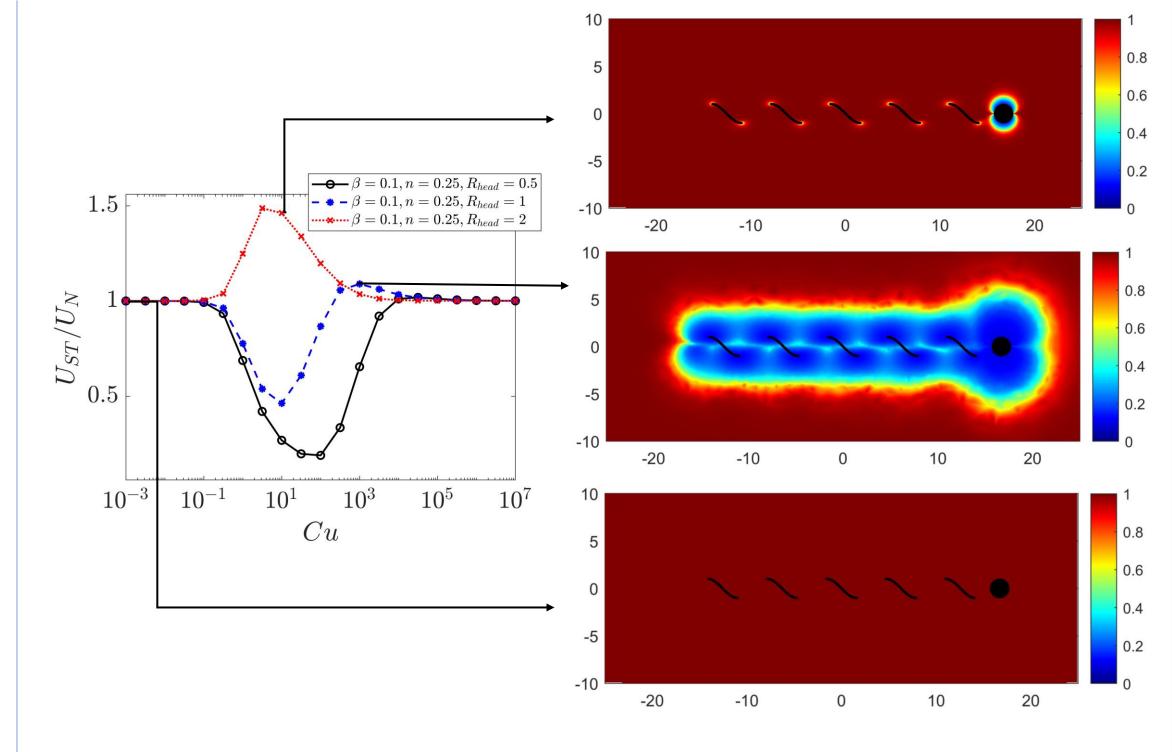




Results



- Carreau model converges to Newtonian results at n=1 as expected
- There is an optimum head size that maximizes velocity. $\mathbf{U} = \mathbf{U}(R_{head}, Cu, n)$
- Lower n (more shear-thinning) yields higher swimming velocities
- Tail efficiency is enhanced overall consistent with literature [2], but head efficiency (and total efficiency) enhancement is size dependent



- ➤ Both enhanced and reduced **U** may be obtained compared to swimming in Newtonian fluids
- Soft confinement effect is observed and contributes to enhanced velocity
- > Swimmer geometry and actuation angular velocity can be tuned to obtain desired results

Future work

Effect of boundaries

- Circulatory system and GI tract are networks of cylindrical channels which will contribute to hydrodynamic interactions
- ? Effect of finite tail length
- Studies focusing on tail geometry consider infinite helical tails
- ? Multiple swimmers
 - Interactions between multiple swimmers may affect the swimming trajectories

References

[1] Pak, O. S., & Lauga, E. (2012). Theoretical models in low-Reynolds-number-locomotion. In *Fluid-Structure Interactions in Low-Reynolds-Number Flows* (1st ed.). Royal Society of Chemistry.

[2] Demir, E., Lordi, N., Ding, Y., & Pak, O. S. (2020). Nonlocal shear-thinning effects substantially enhance helical propulsion. *Physical Review Fluids*, *5*(11), 111301



Acknowledgements





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